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# **Enhancement Method for Augmenting BloodVessels of Retinal Images**

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#### Abstract

Diabetes can cause changes in the blood vessels of the retina, causing them to swell and leak fluid. Diabetic Retinopathy (DR) is a common impediment of diabetes and is the primary cause of preventable blindness. Structural and functional alterations take place in different retinal cells comprising neurons, retinal endothelial cells, and retinal pigment epithelium before clinical symptoms of DR. The appearance of microaneurysms and diabetic macular edema leads to vision loss. The research paper focuses on enhancing the retinal images to detect the occurrence of early symptoms so that the treatment advances in an accurate direction. The research paper demonstrates the enhancement of retinal images obtained from the DRIVE dataset using CLAHE and Morphological methods. The proposed method made use of a Fisher Information matrix and Kalman filter for reducing noise and blurring regions of an image. The vesselness of the retinal images obtained from the DRIVE dataset has been conducted on five scales (0.3, 0.5, 1.0, 1.5, and 2.0) to extract the blood vessels from the retinalimages.

The vesselness is conducted in both RGB and grayscale modes. The obtained ten vesseled images (five colored and five grayscale) are compared with the original input image.

The colored vesseled images are compared with the colored input image and the grayscale vesseled images are compared with the grayscale inputimage. The vesseled image with the highest value of PSNR and lowest value of MSE and RMSE is selected for further processing.

The proposed method makes use of a Histogram Equalization (HE), linear filter, and spatial filter for the removal of noise, and Gamma Transformation for enhancing the retinal images. The percentage of enhancement achieved by the proposed method as compared to CLAHE for MSE, RMSE, and PSNR are 98.23%, 86.81%, and 83.15% respectively, and against morphological operation is 94.93% for MSE, 77.67% for RMSE, and 41.68% for PSNR.

Keywords - CLAHE, Diabetic Retinopathy, DRIVE, PSNR.

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#### I. INTRODUCTION

People suffering from diabetes for an extended time and having poorly controlled blood sugar levels have a higher probability of suffering from Diabetic Retinopathy (DR). DR leads to loss of vision as the blood vessels of the retina undergo gradual destruction. The common symptoms of DR are having a dark spot in the middle of the eyesight, difficulty seeing at night, and blurred vision (Raman et al., 2022). DR is classified into two categories: Non-Proliferative Diabetic Retinopathy (NPDR) and Proliferative Diabetic Retinopathy (PDR). In NPDR, the symptoms are generally non-existent. Due to weakness, the small blood vessels leak blood. The leaked blood or fluid reaches the macula causing it to swell which results in blurred vision. PDR is a progressivestage of the disease. The retina is deprived of oxygen because of circulation impediments. This leads to the coming up of fragile blood vessels that grow in the retina and the back of the eye is filled with gellike fluid (Rom et al., 2022). The newly formed blood vessels leak blood into the center of the eye resulting in blurred eyesight.

The research has been conducted using the retinal images from the Digital Retinal Images for Vessel Extraction (DRIVE) dataset. The DRIVE dataset has a total of 40 colored fundus images in .jpeg format which comprises 7abnormal cases. The source of the images is the diabetic retinopathy screening program in the Netherlands. The Canon CR5 non-mydriatic 3CCD camera with a Field of View (FOV) equal to 45 degrees was used to capture the images. The resolution of each

image is 584\*565 pixels with eight bits per color channel (Nagpal et al., 2022).

The research paper elaborates on the two most popular enhancement techniques used to enhance medical images, Contrast Limited Adaptive Histogram Equalization (CLAHE) and Morphological operations (MOs).

The four MOs (opening, dilation, erosion, and closing) have been analyzed and implemented on the retinal images. Section II discusses the conducted literature review. Section III elaborates on the three performance evaluation metrics: Mean Square Error (MSE), Root Mean Square Error (RMSE), and Peak Signal Noise Ratio (PSNR) with equations and examples. Section IV discusses the two existing enhancement techniques: CLAHE and MOs with their respective flowcharts. Section V elaborates on the proposed method designed and implemented for enhancing the retinal images with a detailed flowchart. Section VI illustrates the implementation of the proposed method. Section VII shows the obtained results followed by Section VIII discussing the conclusion.

# II. LITERATURE REVIEW

The aim of conducting the literature survey is to gather relevant and timely research conducted on the topic chosen for research. The conducted survey needs to be blended into a cohesive summary of existing knowledge in the field. The section presents the conducted literature review in Table 1.

**Table 1. Literature Review** 

References		Models	Performance Evaluation parameters	Datasets	Findings / Results
Hayati et al., 2023	CLAHE, DL (Deep Learning), CNN (Convolutional Neural Network)	(Stochastic Gradient Descent) optimizer	Average accuracy, Training Time, Epoch, Training accuracy, Train loss, Validation accuracy, Validation loss	APTOS 2019	Average Accuracy (original image): VGG16 [87%], InceptionV3 – [90%], Efficient Net – [95%], ResNet34 – [95%] And Average Accuracy (CLAHE): VGG16 [91%], InceptionV3 – [95%], Efficient Net – [97%], ResNet34 – [84%]
Malhi et al., 2023	occurrence	SVM, KNN, DT, Top-hat filtering,		Messidor,	DT tree performs well for grading via microaneurysms with an accuracy of 99.9% whereas SVMand KNN perform well for grading via exudates with an accuracy of 92.1%.

	CLAHE, DL,	MSRCP, LIME, Cycle-	BRISQUE (Blind/Referenceless image spatial quality evaluator), HUE	STARE, CHASEDB1, Proprietary dataset provided by the Affiliated Eye	Proposed DL-based method overcomes the shortcomings of traditional methods, such as color distortion and complex calculations
Mujeeb Rahman et al., 2022		feature	Specificity,	repositories: Kaggle,	The SVM model had a mean AUC of 97.11%, whereas the DNN
			AUC	Zenodo, and	model had a meanAUC of 99.15%
Bataineh & Almotairi, 2021		CLAHE,	PSNR, MSE, SSIM, Entropy	DRIVE, STARE	The proposedmethod achieves the highest accuracy rate for contrast (C) and contrast improvement index (CII) measurements
al., 2021	DL (Deep Learning), AI (Artificial Intelligence)	Denoising (NLMD), GAN	Accuracy, Sensitivity, Specificity, F1- score, IoU, AUC, Cohen's Kappa	Ophtha, IDRiD,	Explored DL in diagnosing DR
Hemanth et al., 2020	DL, HE,CLAHE		Accuracy, Sensitivity, Specificity, Precision, FScore,GMean	MESSIDOR	Accuracy - 97%, Sensitivity - 94%, Specificity - 98%, Precision - 94%, FScore - 94%, and GMean - 95%
2019		color model	PSNR, CNR, Entropy, Histograms, SSIM	DRIVE, MESSIDOR	The proposed method outperformed the existing techniques as per the readings obtained for different performance metrics
Bandara etal., 2018	adaptive contrast enhancement)		TPR, FPR, Accuracy	STARE, DRIVE	The proposed work showed the superiority of SUACE in enhancing retinal images for blood vessel segmentation

		Green Channel,			The proposed method
		Two-stage	CII (Contrast		achieves a better
	HE, CLAHE,	denoising	Improvement Index),	DRIVE,	performance on
Dai et al.,	Normalized	method, Fourth	Linear Index of	STARE,	enhancing retinal
2016	convolution with a	order	Fuzziness, Average	DIARETDB1	fundus image
	domaintransform	PDEs, Median	Running Time		comparing
		filter			with the othermethods
	SHE (Standard		NPSD (Normalised	DRIVE,	Intensity, Saturation,
Shome &	Histogram		Power Spectral	Southern	and noise amplification
Vadali, 2011	Equalization),	Median filter	Distribution), CPS	California	issues are addressed
	CLAHE		(Cumulative Power	College of	
			Spectra)	Optometry	

#### III.PERFORMANCE EVALUATION METRICS

The performance evaluation parameters are the quantifiable and significant measure used for evaluating theperformance of algorithms. The research work made use of three such parameters mentioned as

under.

#### A. MSE (Mean Square Error)

The MSE signifies the cumulative squared error between the compressed and the original image.

$$\frac{1}{n} \sum_{i=1}^{n} (Y_i - \hat{Y}_i)^2$$

Where

- \*n is the number of data points
- $*Y_i$  represents observed values
- $*\hat{Y}_i$  represents predicted values

# B. RMSE (Root Mean Square Error)

RMSE is a square root of MSE. It is used to calculate the variance between the source image and the segmentedimage. The lower the value of RMSE, the better the segmentation performance.

 $RMSE = [MSE]^{1/2}$ 

# C. PSNR (Peak Signal Noise Ratio)

PSNR is a universally used image processing function for comparing two images. PSNR is defined as a proportion between the determined power of an image and the power of noise hindering the quality of its representation. It is the most basic approximation of the difference between two images and is grounded on MSE. The PSNR is calculated by comparing the image with a perfectly clean image.

 $PSNR = 10 \log_{10}[(L-1)^2/MSE]$ 

Where

L – Number of maximum intensity levels

MSE – Mean Square Error

The higher value of the PSNR between two images indicates the greater closeness of the two images. If the two images are exactly similar to each other, the PSNR in such a case is infinity. As PSNR is a logarithmic scale, even minor improvements are enough. PSNR is intended to monitor the removal of noise.

Consider an example to calculate MSE, RMSE, and PSNR. Let's have an original array of 1\*4 say [3 4 15 10] and a reconstructed array [3 5 17 9] and assume that the maximum value for each element is 35. The MSE for the reconstructed array is the mean difference between the original and reconstructed arrays and is

calculated as

 $MSE = \Sigma[(3-3)^2 (4-5)^2 (15-17)^2 (10-9)^2]$ 

 $MSE = \Sigma[0 \ 1 \ 4 \ 1] = 6/4 = 1.5$ 

 $RMSE = [1.5]^{1/2} = 1.2247$ 

 $PSNR = 10*log_{10} (35^2 / MSE) = 10[2log_{10} (35) - log_{10}]$ 

(1.5)] = 29.12044

# IV.PRELIMINARIES

#### A. CLAHE

CLAHE divides the images into relative regions and implements Histogram Equalization to each partition. CLAHE evens out the distribution of used grey values and highlights the hidden features of the images. CLAHEis different from ordinary AHE because it tends to limit contrast. CLAHE implements a clipping limit for addressing the matter of noise amplification. CLAHE restricts the augmentation by clipping the histogram at a predefined value called CDF (Cumulative Distribution Function) [16]. CLAHE splits an input image into non- overlapping contextual areas referred to as blocks or tiles. The two parameters governing the image quality in CLAHE are BS (Block Size) and CL (Clip Limit). On increasing the CL, the brightness of the image increases as the image is of low intensity and the higher CL makes the histogram flatter. On increasing the BS, the contrast of the image increases with the expansion in the dynamic range. These two parameters at the point of maximum entropy curvature generate an image of good quality when using image entropy. Fig. 1 shows the approach adopted to apply CLAHE to enhance the retinal images. The retinal image from the DRIVE dataset is taken as input. The spatia filter is applied to the input image to remove the noise from the image. After the removal of the noise, the highest and lowest pixel values of the image are obtained. The image is then converted to grayscale. Thereafter, padding is conducted on the image to create space around the content of elements within the

boundaries which allows for a more accurate analysis of the image [17]. The pixel count is computed for each contextual area and the values of performance evaluation metrics like PSNR, MSE, and RMSE are calculated between the input and enhanced image.

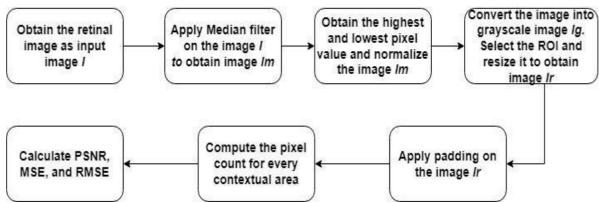


Fig. 1 Methodology for implementing CLAHE

#### B. Morphological Operations (MOs)

The basic components of the MOs are the image and the SE (Structuring Element). The SE is smaller than the image and slides over the image to alter it and generate an image of identical size. There are four different morphological operations mentioned below.

- Dilation Dilation results in creating objects larger in size. It broadens the foreground pixels having a value of 1 and contracts the background pixels having a value of 0. The pixel having a value of 1 in the neighboring is set to 1.
- Erosion Erosion results in creating objects smaller in size. It broadens the background pixels having avalue of 0 and contracts the foreground pixels having a value of 1. The pixel having a value of 0 in the neighboring is set to 0.

- Opening In the opening, the image is first eroded followed by dilation. Opening preserves the shape and size of the larger objects eradicating the smaller objects from the image.
- Closing In closing, the image is first dilated followed by erosion. Closing preserves the shape and size of the objects and fills the small holes in the image. Fig. 2 depicts the methodology obtained for implementing the MOs on the retinal images of the DRIVE dataset. Consider an input image and convert it to grayscale. Perform the four MOs on the image to obtain four output images. Compare each output image with the input image and calculate the performance evaluation metrics. Look for the case with the highest PSNR and lowest MSE and RMSE to find the best among the four operations.

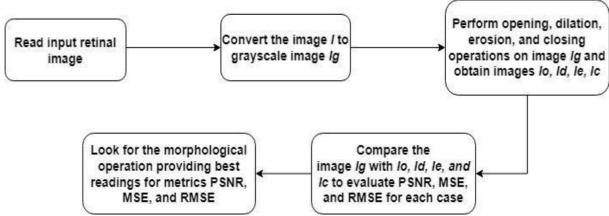


Fig. 2 Methodology for implementing Mos

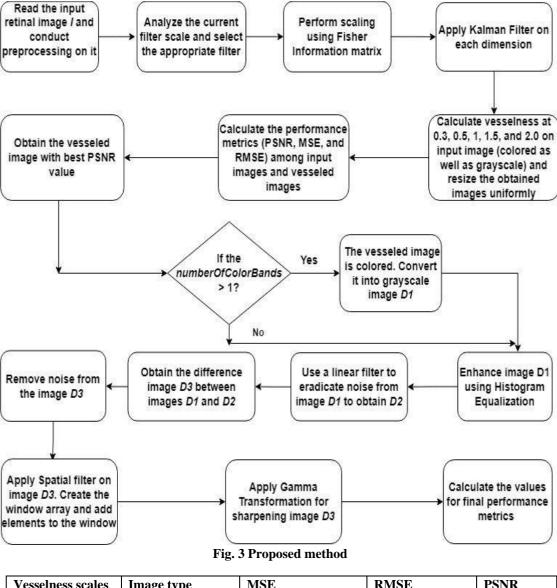
#### V. CONTRIBUTION

Fig. 3 shows the proposed method for enhancing the retinal images. The proposed method made use of a Fisher Information matrix and Kalman filter. The Fisher information is a method of determining the amount of information that a noticeable random variable X transfers about an unidentified parameter  $\theta$  upon which the probability of X depends. Kalman filter

uses a sequence of measurements perceived over time comprising statistical noise and other inconsistencies to generate approximations of unknown variables that incline to be more precise than those grounded on a single measurement alone by approximating a joint probability distribution over the variables for each timeframe. The vesselness of the retinal images obtained from the DRIVE dataset has been conducted

on five scales (0.3, 0.5, 1.0, 1.5, and 2.0) to extract the blood vessels from the retinal images. The vesselness is steered in both RGB and grayscale modes. The ten obtained vesseled images (five colored and five grayscale) are compared with the original input image. The colored vesseled images are compared with the colored input image and the grayscale vesseled images are compared with the grayscale input image. The vesseled image with the highest value of PSNR and lowest value of MSE and RMSE selected for further processing. The proposed method makes use of a

Histogram Equalization (HE), linear filter, and spatial filter for introducing blurring intended to remove the small details from the image followed by noise reduction, and Gamma Transformation for enhancing the retinal images. The enhancement of the images differs from the variation in the value of  $\gamma$  (gamma). Each display device has its gamma correction which results in displaying the images at different intensities. Fig. 3 shows the detailed flowchart illustrating the research methodology adopted for enhancing the retinal images using the proposed method.



Vesselness scales	Image type	MSE	RMSE	PSNR
0.3	Colored	7.4671	2.7326	30.67
0.5	Colored	9.2789	3.0461	28.78
1.0	Colored	11.9294	3.4539	26.60
1.5	Colored	12.8855	3.5896	25.93
2.0	Colored	9.2789	3.0461	28.78

#### VI.IMPLEMENTATION

Fig. 4 shows the images obtained after applying vesselness at five levels (0.3, 0.5, 1.0, 1.5, and 2.0).

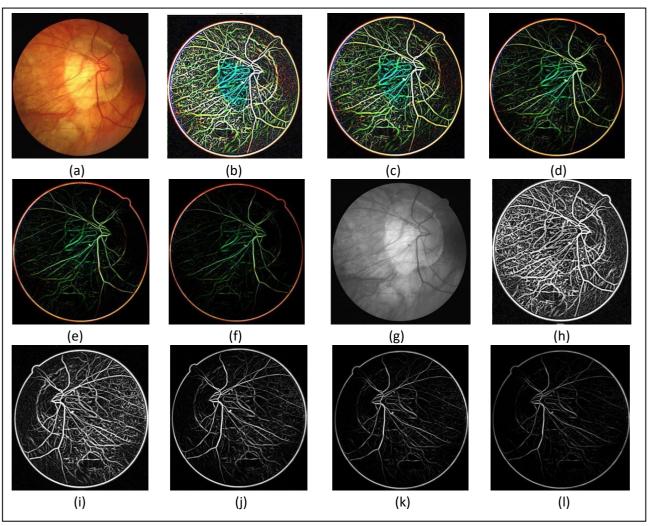


Fig. 4 (a) Colored Input image (b) Colored vesseled image at 0.3 (c) Colored vesseled image at 0.5 (d) Colored vesseled image at 1.0 (e) Colored vesseled image at 1.5 (f) Colored vesseled image at 2.0 (g) Grayscale input image (h) Grayscale vesseled image at 0.3 (i) Grayscale vesseled image at 0.5 (j) Grayscale vesseled image at 1.0 (k) Grayscale vesseled image at 1.5 (l) Grayscale vesseled image at 2.0

Table 2 shows the reading of performance evaluation metrics obtained after comparing the five different scales of vesselness with the input image. The colored input image is compared with the colored vesseled images and the grayscale input image is compared with the grayscale vesseled image.

0.3	Grayscale	10.2991	3.2092	27.87
0.5	Grayscale	11.9272	3.4536	26.60
1.0	Grayscale	4.1119	2.0278	35.85
1.5	Grayscale	13.5314	3.6785	25.50
2	Grayscale	13.6240	3.6911	25.44

The best results have been obtained for vesselness conducted at scale 1 for grayscale images with PSNR of highest PSNR of 35.85 dB and lowest values of MSE of 4.1119 and RMSE of 2.0278 respectively.

The vesseled grayscale image at scale 1.0 is provided as input to the proposed model. Firstly, the vesseled image is normalized to obtain image *D1* as shown in Fig. 5(a)

followed by the removal of noise from the retinal image using a Kalman filter as in Fig. 5(b). The image is enhanced using the adaptive filter to obtain image D2 as in Fig. 5(c). Thereafter the difference image is obtained after subtracting D1 from D2 as in Fig. 5(d). Finally, the Gamma Transformation is applied to the different images to obtain the image in Fig. 5(e).

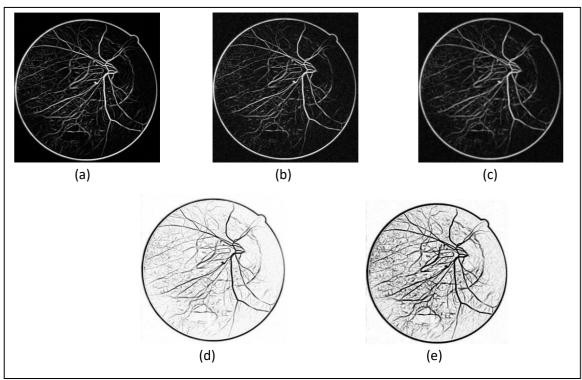


Fig. 5 (a) Normalized vesseled image D1 (b) Removal of noise using Kalman filter (c) Enhanced image after applying filters D2 (d) Difference image (D1-D2) (e) Gamma Transformation applied on the difference image.

The readings of the three performance metrics obtained after applying the proposed method are mentioned below.

MSE - 0.3035

RMSE - 0.5509

PSNR - 58.49 dB

# VII. RESULTS

This section elaborates on the results obtained for each of the three approaches used to enhance the retinal images in the

DRIVE dataset. Table 3 shows the MSE, RMSE, and PSNR values for 20 retinal pictures from the DRIVE dataset.

Image name	Input Image	MSE	RMSE	PSNR (dB)	Output image
21_training.pgm		6.3487	2.5197	32.08	
22_training.pgm		6.3649	2.5229	32.05	
23_training.pgm		6.3010	2.5102	32.14	
24_training.pgm		6.1486	2.4796	32.36	
25_traning.pgm		7.5986	2.7566	30.52	
26_training.pgm		8.3806	2.8949	29.67	
27_training.pgm		6.2659	2.5032	32.19	
28_training.pgm		6.4131	2.5324	31.99	

29_training.pgm	7.9348	2.8169	30.14	
30_training.pgm	8.3125	2.8831	29.74	
31_training.pgm	5.2645	2.2945	33.70	
32_training.pgm	6.3762	2.5251	32.04	
33_training.pgm	6.3432	2.5186	32.08	
34_training.pgm	7.5347	2.7449	30.59	
35_training.pgm	7.2688	2.6961	30.90	
36_training.pgm	7.3629	2.7135	30.79	
37_training.pgm	6.8943	2.6257	31.36	

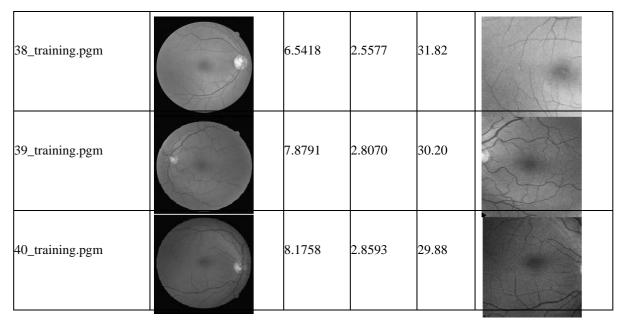


Table 4 illustrates the performance data acquired for four MOs. The MSE, RMSE, and PSNR values are determined for 20 retinal images from the DRIVE dataset for each MO, and it is discovered that dilation outperformed the other three operations on all 20 images. As a result, among the four MOs, dilation operation readings are the most precisely recorded.

		Openi	ing		Dilate	d		Erode	d		Closin	ıg		
Image name (*.pgm )	Inputimage	MSE		PS N R			PS N R	MSE		PS N R	MSE			Output image
21_trai ning		5.5 312									5.5 312		33. 27	
22_trai ning		4.8 145									4,8 145	1	34. 48	
23_trai		5.2 379						5.0 351			5.2 379		33. 75	
24_trai ning		4.5 606									4.5 606		34. 95	J
25_tran ing		4.5 537					42. 65				4.5 537		34. 96	
26_trai ning		4.1 101						3.8 655	1.9 661	36. 39	4.1 101		35. 85	

27_trai ning	4.8 190	2.1 952	34. 47	2.6 690	1.6 337	39. 60	4.6 740	2.1 619	34. 74	4.8 190	2.1 952	34. 47	
28_trai ning	7.7 437	2.7 827	30. 35	3.0 767	1.7 541	38. 37	7.2 096	2.6 851	30. 97	7.7 437	2.7 827	30. 35	
29_trai ning	6.9 335	2.6 332	31. 31	2.9 531	1.7 185	38. 73	6.4 851	2.5 466	31. 89	6.9 335	2.6 332	31. 31	3
30_trai ning	3.9 669	1.9 917	36. 16	2.1 169	1.4 550	41. 62	3.8 538	1.9 631	36. 41	3.9 669	1.9 917	36. 16	
31_trai ning	6.1 602	2.4 820	32. 34	2.4 681	1.5 710	40. 28	5.9 456	2.4 384	32. 65	6.1 602	2.4 820	32. 34	
32_trai ning	4.8 288	2.1 975	34. 45	1.8 897	1.3 747	42. 60	4.5 125	2.1 243	35. 04	4.8 288	2.1 975	34. 45	
33_trai ning	5.2 850	2.2 989	33. 67	1.9 390	1.3 925	42. 38	5.1 150	2.2 616	33. 95	5.2 850	2.2 989	33. 67	
34_trai ning	7.0 257	2.6 506	31. 20	2.3 106	1.5 201	40. 86	6.7 449	2.5 971	31. 55	7.0 257	2.6 506	31. 20	
35_trai ning	5.5 577	2.3 575	33. 23	2.6 051	1.6 140	39. 81	5.4 015	2.3 241	33. 48	5.5 577	2.3 575	33. 23	
36_trai ning	5.6 640	2.3 799	33. 07	2.2 457	1.4 986	41. 10	5.4 505	2.3 346	33. 40	5.6 640	2.3 799	33. 07	
37_trai ning	6.4 337	2.5 365	31. 96	2.7 967	1.6 723	39. 20	6.3 551	2.5 209	32. 07	6.4 337	2.5 365	31. 96	
38_trai ning	5.1 724	2.2 743	33. 86	2.5 262	1.5 894	40. 08	5.1 007	2.2 585	33. 98	5.1 724	2.2 743	33. 86	
39_trai ning	4.8 163	2.1 946	34. 48	2.6 543	1.6 292	39. 65	4.6 754	2.1 635	34. 73	4.8 163	2.1 946	34. 48	
40_trai ning	4.9 438	2.2 235	34. 25	2.4 116	1.5 529	40. 48	4.7 908	2.1 888	34. 52	4.9 438	2.2 235	34. 25	

Table 5: displays the results of the performance metrics acquired for the proposed technique. MSE, RMSE, and PSNR values were calculated for 20 retinal images from the DRIVE dataset, and it was discovered that for all 20 images, the readings of all performance metrics are higher than the readings obtained in Table 3 for CLAHE and Table 4 for MOs. The proposed technique outperformed both CLAHE and MOs in improving retinal

		im	ages.		
Image name	Input Image	MSE	RMSE	PSNR(dB)	Output image
21_training.tif		0.1347	0.3670	56.83	
22_training.tif		0.1075	0.3279	57.81	
23_training.tif		0.1032	0.3212	57.99	
24_training.tif		0.1107	0.3327	57.69	
25_traning.tif		0.1063	0.3260	57.86	
26_training.tif		0.1361	0.3689	56.79	
27_training.tif		0.0964	0.3104	58.29	

28_training.tif	0.1534	0.3917	56.27	
29_training.tif	0.1241	0.3523	57.19	
30_training.tif	0.1097	0.3312	57.73	
31_training.tif	0.0875	0.2958	58.71	
32_training.tif	0.1589	0.3986	56.11	
33_training.tif	0.1364	0.3693	56.78	
34_training.tif	0.0563	0.2373	60.62	
35_training.tif	0.1544	0.3929	56.24	

36_training.tif	0.1489	0.3858	56.40	
37_training.tif	0.1636	0.4045	55.99	
38_training.tif	0.0834	0.2888	58.92	
39_training.tif	0.1324	0.3639	56.91	
40_training.tif	0.1658	0.4071	55.93	

# VIII. CONCLUSION

The higher the PSNR number and the lower the MSE and RMSE values, the greater the degree of improvement accomplished. The average MSE and RMSE for CLAHE are 6.9855 and 2.6430, respectively, which are the highest. The proposed technique achieves the lowest MSE and RMSE values (0.1235 and 0.3487, respectively). The dilation operation achieves the lowest MSE and RMSE among the MOs, at 2.43852 and

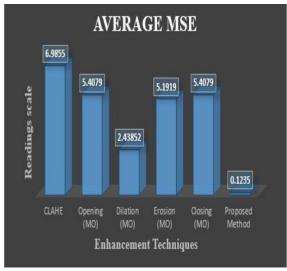
1.5616, respectively. The proposed technique achieved the maximum PSNR of 57.35 dB, outperforming the CLAHE and MOs. The CLAHE has the lowest average PSNR (31.312). The best average PSNR for dilation operations is

40.477 dB, while the lowest average PSNR for opening and closure operations is 33.603. The results in Table 6 show that the suggested method outperformed existing ways of improving retinal images in all operations.

Table 6. Comparative mean values of performance metrics for CLAHE, MOs, and proposed method

Average MSE		Average RMSE	Average PSNR
CLAHE	6.9855	2.6430	31.312
Opening (MO)	5.4079	2.3254	33.603
Dilation (MO)	2.4385	1.5616	40.477
Erosion (MO)	5.1919	2.2785	33.95
Closing (MO)	5.4079	2.3255	33.603
Proposed Method	0.1235	0.3487	57.35

Fig. 6, 7, and 8 show the graphical representation of average MSE, average RMSE, and average PSNR respectively. The proposed method has the lowest average MSE and RMSE and the highest value of average PSNR.



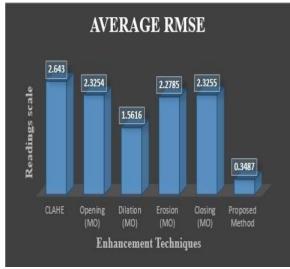


Fig. 6 Average MSE

Fig. 7 Average RMSE



Fig. 8 Average PSNR

The percentage of enhancement achieved by the proposed method as compared to CLAHE and MO (dilation) is shown in Table 7. As dilation provided the

best results for the performance evaluation metrics as shown in Table6, so in MOs only dilation is compared with the proposed method.

Table 7. Percentage of enhancement achieved

Enhancement percentage	MSE	RMSE	PSNR
CLAHE and Proposed method	98.23%	86.81%	83.16%
MO (dilation) and Proposed method	94.93%	77.67%	41.68%

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